

available at www.sciencedirect.comjournal homepage: www.ejconline.com

A simulation study to evaluate the impact of the number of lesions measured on response assessment

Chaya S. Moskowitz^{a,*}, Xiaoyu Jia^a, Lawrence H. Schwartz^b, Mithat Gönen^a

^aDepartment of Epidemiology and Biostatistics, Memorial Sloan-Kettering Cancer Center, 307 East 63rd Street, 3rd Floor, NY 10065, United States

^bDepartment of Radiology, Memorial Sloan-Kettering Cancer Center, 1275 York Avenue, NY 10065, United States

ARTICLE INFO

Article history:

Received 4 November 2008

Accepted 7 November 2008

Available online 16 December 2008

Keywords:

Cancer imaging

Ct imaging

Inter-reader variability

Random effects model

RECIST criteria

Response to therapy

ABSTRACT

The objectives of this study were to evaluate whether the number of lesions that are used to measure tumour burden affects response assessment and inter-rater variability. In order to accomplish this, a simulation study was conducted. Data were generated from a mixed-effects mixture model. Parameter values to input in the model were obtained from the analysis of real data. Response assessments based on 10, five, three, two and one lesion were evaluated. There was little difference between response assessments based on five lesions and response assessments based on 10 lesions. When fewer than five lesions were used to assess response, there were notable differences from the 10 lesion-based response assessment. Basing response assessment on a small number of lesions tends to overestimate response rates and leads to misclassification of patients' response status. Therefore, measuring five lesions per patient appears to sufficiently capture patients' response to therapy. Measuring fewer than five lesions results in the loss of information that may adversely affect clinical trial results as well as patient management.

© 2008 Elsevier Ltd. All rights reserved.

1. Introduction

Response to chemotherapy is an essential part of patient care and clinical research. Responding patients are often offered prolonged treatment and non-responders are quickly switched to another treatment regimen. Phase II clinical trials using response as the primary end-point are ubiquitous and often are the primary determinants of whether a regimen should be taken to a definitive Phase III study. Hence, accurate determination of response to chemotherapy is of critical importance.

Patients who receive treatment for cancer, whether as participants in a clinical trial or simply in the course of standard therapy, usually have multiple sites of metastases, in multiple organs. It is possible that the effect of the treatment will not be identical at all sites of metastases. For example, the treat-

ment may shrink all the lesions but by varying degrees (Fig. 1). In some instances, it is even possible for certain lesions to shrink in response to treatment whilst others grow. When assessing response to therapy, such as with RECIST guidelines,¹ it might therefore seem necessary to measure all lesions in order to best evaluate completely whether a patient is responding to a therapy. In fact, there is some empirical evidence in the literature that the variability in tumour response measurements is substantially reduced, as increasing numbers of lesions are measured.² Often, however, resources do not permit radiologists to evaluate every lesion, and instead a subset or selection of lesions is chosen. The original WHO criteria recommended that five lesions be measured.^{3,4} In the RECIST 1.0 guidelines, recommendations were for measuring all lesions up to a total of 10. In patients with more than 10 lesions, the choice of which lesions to measure

* Corresponding author: Tel.: +1 (646) 735 8117; fax: +1 (646) 735 0010.

E-mail address: moskowc1@MSKCC.ORG (C.S. Moskowitz).
0959-8049/\$ - see front matter © 2008 Elsevier Ltd. All rights reserved.
doi:10.1016/j.ejca.2008.11.010

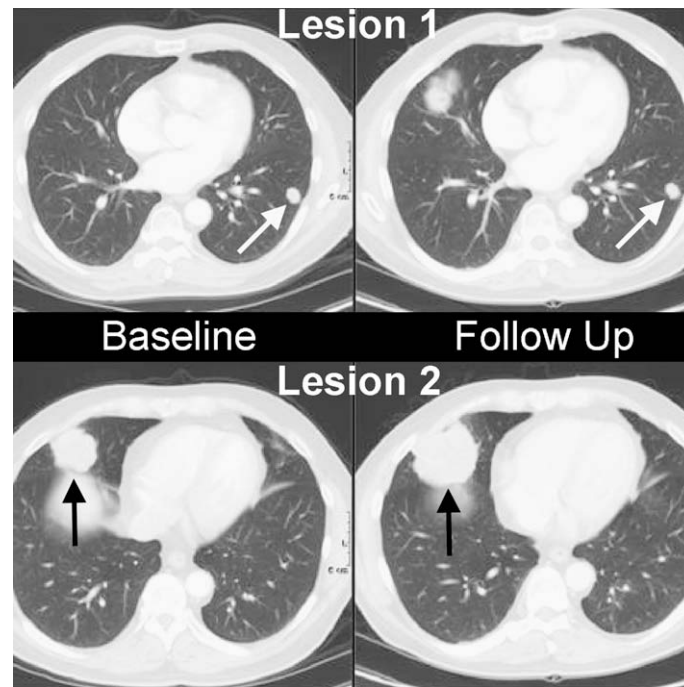


Fig. 1 – Metastatic disease to the lungs. Note that the smaller lesion (white arrows) has not changed in size from baseline to follow-up, whilst the larger lesion (black arrows) has increased in size.

should be based on the size of the lesion and how suitable it is for repeated measurements.

In practice, measuring up to an upper limit of 10 lesions may still be difficult and require more time and effort than many radiologists are routinely able to devote. A natural question to ask is whether fewer lesions can be measured whilst still sufficiently capturing a patient's response to therapy. If so, how many lesions must one measure?

A key difficulty in answering this question is that the truth is rarely, if ever, known. In order to know whether a radiologist's repeated assessments of tumour burden accurately reflects a patient's change in true tumour burden over the course of a therapy, after being imaged at each time point the patient would need to undergo surgery and have all of their lesions measured. Clearly this is not possible.

One potential way to address this issue is to compare the response assessment that would have been obtained had we measured fewer than 10 lesions with the response assessment obtained based on the complete 10 lesions. In some sense, this approach considers the response assessment based on the 10 lesions to be the gold standard. It must be acknowledged, however, that response assessment based on the 10 lesions is not necessarily 'the truth.' Unmeasured lesions beyond this upper limit may change the assessment. With this caveat in mind, comparing a 10 lesion-based response assessment with a response assessment based on fewer lesions would help answer the question of whether measuring less than 10 lesions would substantially alter the way tumour burden is currently evaluated under the RECIST 1.0 guidelines.

Another issue to be taken into consideration is that response assessment is radiologist-specific. That is, each radiologist selects what he or she perceives to be the 10 largest lesions and then measures these lesions to the best of their

ability. Inter-rater variability in this setting, however, is not inconsequential and whether a patient is determined to have responded to treatment may in fact differ between radiologists.^{5,6} We might further question, then, whether radiologists are more likely to agree in their response assessments if they measure more lesions. It seems logical to be most comfortable with response assessments that have a high level of agreement between multiple radiologists.

In this journal, the paper entitled 'Individual patient data analysis to assess modifications to the RECIST criteria' evaluates the EORTC data warehouse⁷ and assesses change in response by decreasing the number of lesions. There was concern that this database collated from both industrial trials and cooperative group trials may not be truly representative of total tumour burden and number of lesions. In fact the mean number of lesions in those cooperative group trials was approximately 40% lower than the industrial independently reviewed trials. Therefore, part of the rationale of this simulation study is to more precisely approximate total tumour burden.

There are several advantages to conducting a simulation study including the ability to change the parameter settings that are used to simulate the data and the ability to explore the results in a variety of scenarios. For these reasons, we undertook this simulation study.

2. Methods

The primary aim of this simulation study was to evaluate whether the number of lesions measured affects response assessment. Secondly, we were also interested in exploring whether the number of lesions measured affects inter-rater variability.

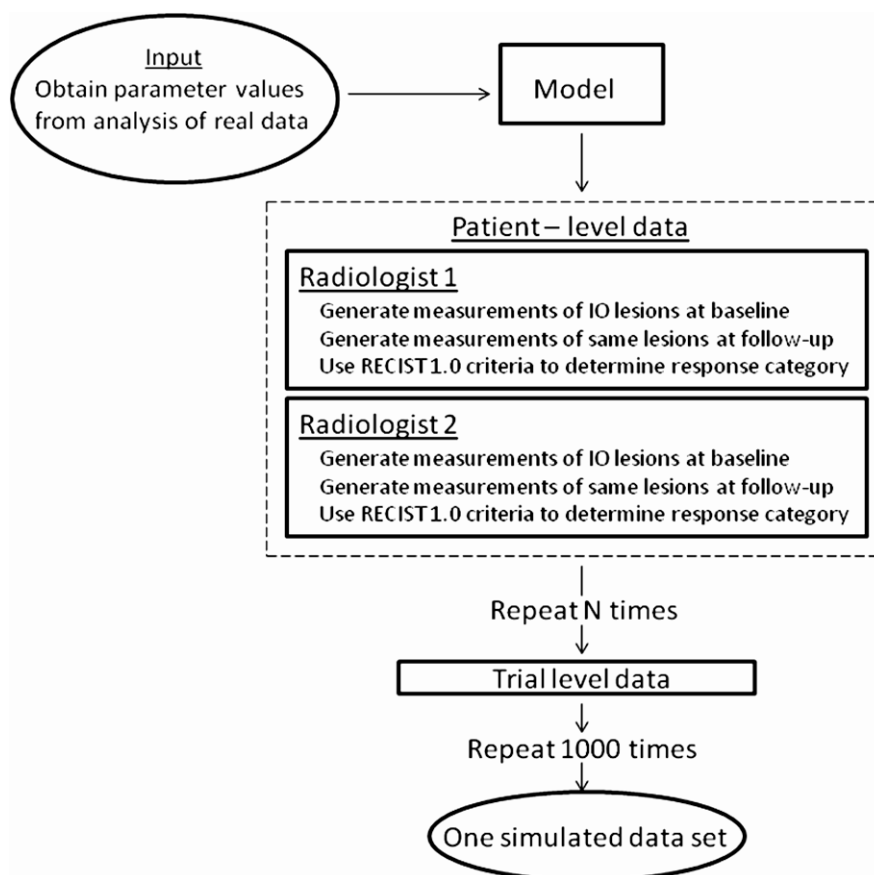


Fig. 2 – Flowchart of the simulation process.

The flowchart in Fig. 2 portrays how data were simulated. Our general approach was to generate measurements on 10 lesions for each patient in hypothetical single-arm trials at two time points (before and after treatment). Based on the change in lesion size between the two time points, we determined each patient's response as per RECIST 1.0 guidelines, first using all target lesions and then using only a subset of each patient's largest lesions. By varying the number of target lesions in the subset, we could assess the effect of the number of lesions measured. In addition, at each time point we generated two lesion measurements to simulate two radiologists reading each image. In all the scenarios we studied, we repeated this process 1000 times to simulate 1000 trials. For the interested reader, the Appendix describes the simulation model and provides a detailed description of how data were generated.

3. Results

3.1. Description of simulated data

To better understand the results, it is helpful to have an idea of what the simulated data actually look like. To this end, we first give an example of the lesion measurements generated for individual patients.

Fig. 3 shows lesion measurements from two simulated patients who responded to therapy. The first row contains a patient whose lesion measurements were generated as part of a

trial with a low response rate, whilst the second row contains a patient who was generated as part of a trial with a high response rate. The first figure in each row corresponds to measurements made by the first radiologist, and the second figure corresponds to the repeated reading by the second radiologist. The darker shaded bar depicts the baseline measurement of a lesion, whilst the adjacent lighter colour bar depicts the follow-up measurement after therapy.

In the first plot, we see a patient for whom the first radiologist measured a decrease in lesion size for all the 10 lesions. Whilst the decreasing trend is consistent across the 10 lesions, the lesions decrease in varying degrees. The second plot in the top row shows the second radiologist's measurements of the same lesions. There is a similar tendency for all the lesions to decrease in size here as well, although the measurements themselves differ somewhat from those made by the first radiologist. In contrast to the first patient, most but not all the 10 lesions in the second patient (shown in the bottom row) are judged by the first radiologist to be shrinking. Some of the lesions regress considerably, whilst other lesions remain unchanged or even appear to grow slightly. Again, an identical trend is seen from the measurements made by the second radiologist, but the actual measurements made by the two radiologists differ.

Fig. 4 again shows lesion measurements for individual patients except here the top row displays measurements generated for a patient with progressive disease (top row) and a patient with stable disease (bottom row). For the patient with

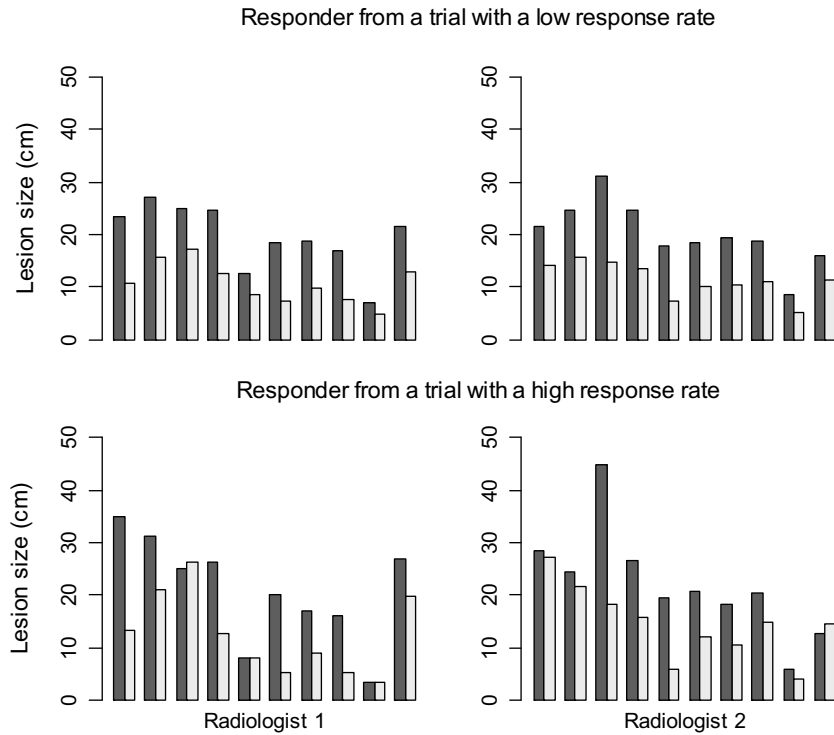


Fig. 3 – An example of 10 lesion measurements at baseline (shaded bar) and follow-up (light bar) for two sample patients who were classified as responders.

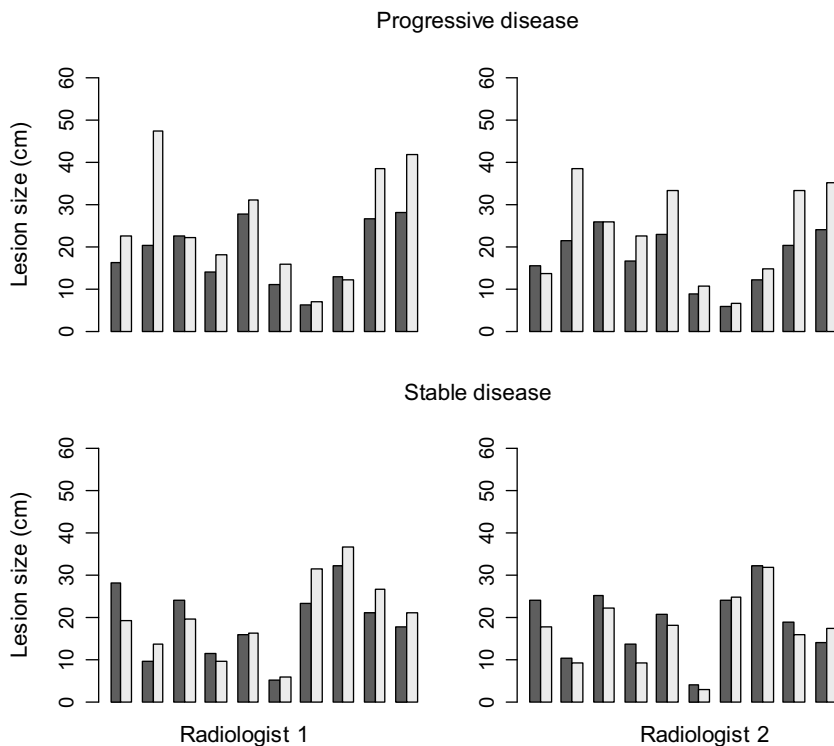


Fig. 4 – An example of 10 lesion measurements at baseline (shaded bar) and follow-up (light bar) for a patient with progressive disease and a patient with stable disease.

progressive disease, the measurements made by both radiologists show an increase in lesion size for the majority of le-

sions with one or two lesions (depending on the radiologist) decreasing very slightly in size. For the patient with stable

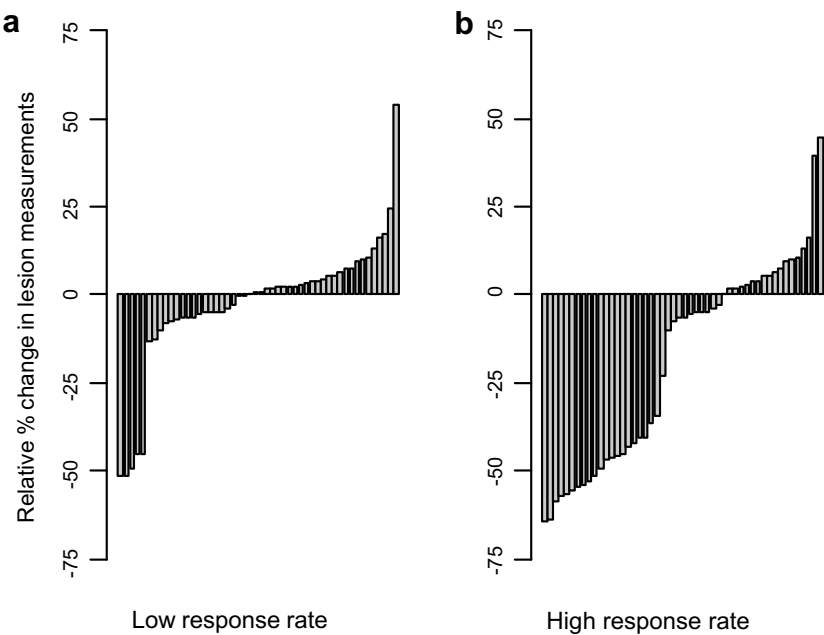


Fig. 5 – Waterfall plots for a single simulated Phase II study with a low response rate and a single simulated Phase II study with a high response rate.

disease, some lesions increase whilst others decrease in size, but the change in measurements is relatively small in all cases.

To depict the data for an entire simulated clinical trial, in Fig. 5 we present waterfall plots for a single trial with a low response rate and another trial with a high response rate. In both cases, we used a trial with $N = 50$ patients and give the measurements from only one radiologist. The waterfall plots show the percent relative change in total tumour size for each patient.

3.2. Response and progression rates

To summarise the results across 1000 simulated trials, we began by estimating the response and progression rates in each trial and then averaging these rates across the 1000 trials. The response rate was calculated by combining complete and partial responders as is frequently done in Phase II studies and then dividing by the number of patients in the trial ($(CR + PR)/N$, where N is the number of patients in the trial). The progression rate was calculated by dividing the number of patients with progressive disease by the total sample size (PD/N). In each trial we estimated response and progression rates separately for each radiologist. Agreement between the radiologists was calculated for each trial using the proportion of overall agreement⁸ based on a 2×2 table of either responders \times non-responders or progressors \times non-progressors. We report the average of this proportion of agreement across the 1000 trials. Results of these analyses are shown in Tables 1–4.

Starting with Table 1, the first row shows the average response rates for trials with 25 patients assuming that all 10 lesions are included in the response assessments. For both radiologists, we see an 8% average response rate across the

Table 1 – Low response: average response rates across 1000 simulated trials.				
N	Number of lesions measured	Response rate (%) Radiologist		Overall proportion of agreement
		1	2	
25	10	8	8	>0.99
	5	8	8	>0.99
	3	10	10	0.96
	2	13	13	0.90
	1	22	22	0.76
50	10	10	10	>0.99
	5	10	10	>0.99
	3	12	12	0.96
	2	16	15	0.90
	1	24	24	0.76
100	10	10	10	>0.99
	5	10	10	0.99
	3	12	12	0.96
	2	15	15	0.90
	1	24	24	0.76

trials. Furthermore, there is a very high level of agreement between the two radiologists when all lesions are considered. In the next row, the same patients are analysed in each trial, but now only the five largest target lesions are included in the assessments. These results are virtually identical to when all 10 lesions are used. The response rates are again 8% for both radiologists, and there is a very high level of agreement between the radiologists. In the third row, only the three largest lesions are considered in the response assessment. Here, we see that the average response assessments now increase to 10%. The overall proportion of agreement drops slightly

Table 2 – Low response: average progression rates across 1000 simulated trials.

N	Number of lesions measured	Progression rate (%) Radiologist		Overall proportion of agreement
		1	2	
25	10	4	4	0.97
	5	3	4	0.96
	3	4	5	0.93
	2	6	6	0.90
	1	10	10	0.83
50	10	4	4	0.98
	5	4	3	0.96
	3	4	4	0.93
	2	6	6	0.91
	1	9	9	0.85
100	10	3	4	0.98
	5	3	4	0.96
	3	4	4	0.94
	2	6	6	0.91
	1	9	9	0.85

from what was seen for 10 and five lesions, but is still very high. In looking at the next two rows, the estimated response rates based on the two lesions and one lesion continue to increase, whilst the proportion of agreement between the radiologists continues to decrease relative to what was seen for the rates based on all the 10 lesions. The additional rows in Table 1 show similar results when the trials have 50 patients and 100 patients. On average, we estimate the same response rates for 10 lesions and five lesions with very high levels of agreement between the two radiologists. When the number of lesions considered is reduced to three or fewer lesions, we see the average response rates increase and the agreement between the radiologists decreases. In the case of three lesions, differences relative to a 10 lesion-based assessment are noticeable, but rather small. In the situation when only the largest lesion is considered, these differences become quite substantial.

In Table 2, the same simulation sets are analysed except now the focus is on the progression rate. Based on the response assessment using 10 lesions, the average progression rate across the different scenarios (sample sizes and radiologists) is 4%. Small differences of 1% are seen, when the number of lesions evaluated is decreased to either five or three lesions. The agreement between the radiologists is very high when 10 lesions are used. It is relatively similar when five lesions are used, but begins to decrease slightly when only three lesions are used. When fewer than three lesions are evaluated, the estimated progression rate increases and the agreement between the radiologists decreases even further.

Tables 3 and 4 are similar to Tables 1 and 2, except here data were simulated to have a high response rate of slightly over 40%. A trend comparable to that seen in Tables 1 and 2 is found here as well. With the response assessment based on the 10 lesions as the reference, using five lesions yields identical response and progression rates. Using three lesions produces similar but not uniformly identical estimates. More

variation between the estimates arises if only two or one lesion is considered. The agreement between the radiologists decreases as the number of lesions evaluated decreases.

3.3. Discordant patient-level response assessment

To further analyse the simulation results, we calculated the proportion of patients whose response assessment changed based on the number of lesions that are assessed. For this purpose we used binary assessments, i.e. responder versus non-responder (CR + PR versus SD + PD), and then separately progressor versus non-progressor (PD versus CR + PR + SD). Within each trial, we estimated the proportion of patients with discordant assessments depending on how many lesions were included in the assessment. For instance, we compared five lesions with 10 lesions by counting the number of patients who were classified as responders using a 10 lesion-based assessment and non-responders using a five lesion-based assessment plus the number of patients who were classified as non-responders using a 10 lesion-based assessment and responders using a five lesion-based assessment. This number was divided by the number of patients in the trial and then the result was averaged over the 1000 trials in the simulation set. This computation was repeated for all pair-wise comparisons of 10, five, three, two and one lesion. Tables 5–8 contain these results.

In Table 5 we see that when the therapy has a low response rate, for both radiologists on average less than 1% of patients are reclassified as either responders or non-responders based on whether 10 or five lesions are measured. This result holds regardless of the sample size used. Depending on whether 10 lesions or three lesions are measured, approximately 2% of patients have their response status changed. This number increases to 6% when comparing 10 lesions with two lesions, and 15% when comparing 10 lesions with the single largest lesion.

Table 6 shows that on average 2% of patients are reclassified as having progressive disease or not depending on whether 10 lesions or five lesions are measured. As fewer lesions are considered, the proportion of patients found to have discordant progression assessments increases.

Table 7 shows results similar to Table 5 when the therapy has a high response rate. The results are very similar to what was seen in Table 5. Similarly, Table 8 is comparable to Table 6.

4. Discussion

The accurate and reproducible measurement of tumour burden at baseline and follow-up CT scans is of paramount importance in assessing response to therapy. The earliest use of tumour burden and imaging biomarkers mandated that more than one tumour be assessed in a patient. As imaging modalities have improved, so has the ability to detect metastatic disease and smaller changes in these metastases. Nevertheless, there remains the question of what proportion of tumour burden is necessary to assess and measure quantitatively. Actual trial data where ‘all lesions’ are measured are not common, certainly not across multiple primary tumours

Table 3 – High response: average response rates across 1000 simulated trials.

N	Number of lesions measured	Response rate (%) Radiologist		Overall proportion of agreement
		1	2	
25	10	43	43	0.98
	5	43	43	0.98
	3	44	44	0.95
	2	46	46	0.91
	1	50	50	0.81
50	10	43	43	0.98
	5	43	43	0.98
	3	44	44	0.95
	2	46	46	0.91
	1	50	50	0.81
100	10	42	42	0.98
	5	42	42	0.98
	3	43	43	0.95
	2	45	45	0.91
	1	49	50	0.81

Table 4 – High response: average progression rates across 1000 simulated trials.

N	Number of lesions measured	Progression rate (%) Radiologist		Overall proportion of agreement
		1	2	
25	10	3	3	0.98
	5	3	3	0.97
	3	3	4	0.95
	2	4	4	0.94
	1	6	7	0.89
50	10	3	3	0.98
	5	3	3	0.97
	3	3	3	0.95
	2	4	4	0.94
	1	7	7	0.90
100	10	3	3	0.98
	5	3	3	0.97
	3	3	3	0.95
	2	4	4	0.93
	1	7	7	0.89

and types of therapy. Therefore, we sought to evaluate this question with a simulation study whose simulation parameters are based upon actual tumour measurements.

We began by considering the scenario of 10 target lesions per patient and decreasing the number of lesions measured to five, three, two or one, similar to the approach in the RE-CIST data warehouse analysis.⁷

Across all the scenarios that were considered, we consistently saw little or no difference when comparing response and progression assessments based on the five largest target lesions with these assessments based on the 10 target lesions. In some, but not all, situations, agreement between the radiologists decreased very slightly when comparing the five lesion-based assessment with the 10 lesion-based assessment.

The differences in response assessment between 10 lesions and three, two or one lesion were more prominent. It is obvious that measuring a single lesion gives misleading results. In a clinical trial of 50 patients, a typical size for Phase II studies, response rates would be overestimated by 7–14% (Tables 2 and 4). A trial of this size would often be powered to detect a difference of 15–20% in response rates⁹ so this amount of overestimation can easily lead to declaring an ineffective drug promising. The amount of overestimation is 3–6% for two lesions and 1–2% for three lesions. Whilst measuring three lesions represents an improvement over measuring two or a single lesion, the latter figures fall short of our original goal of sufficiently representing patient experience with a smaller number of lesions.

On an individual basis, measuring one to three lesions continues to be less sufficient or insufficient. When compared with 10 lesions, measuring a single lesion causes 11–16% of the patients to be misclassified. With two lesions, this misclassification drops to 5–6% and with three lesions to 2–3%. Measuring five lesions assures that at most 1% (and in many cases less than 1%) of the patients are incorrectly classified.

Another way to evaluate Tables 5–8 is to examine the misclassification rates of measuring one to three lesions as compared with measuring five lesions. Five lesions reduced misclassification rate by 2% in absolute terms when compared with three lesions and by 5–15% when compared with one or two lesions.

The tables demonstrate that measuring smaller number of lesions leads to overstated response rates and a higher proportion of misclassified patients. This is consistently seen

Table 5 – Response classification in trials with a low response rate: proportion of patients classified discordantly into responders and non-responders.

Number of lesions being compared	N = 25		N = 50		N = 100	
	Radiologist 1	Radiologist 2	Radiologist 1	Radiologist 2	Radiologist 1	Radiologist 2
10 versus 5	<0.01	<0.01	<0.01	<0.01	<0.01	<0.01
10 versus 3	0.02	0.02	0.02	0.02	0.02	0.02
10 versus 2	0.06	0.06	0.06	0.06	0.06	0.06
10 versus 1	0.15	0.15	0.15	0.15	0.15	0.15
5 versus 3	0.02	0.02	0.02	0.02	0.02	0.02
5 versus 2	0.05	0.05	0.05	0.05	0.05	0.05
5 versus 1	0.15	0.15	0.15	0.14	0.15	0.14
3 versus 2	0.04	0.04	0.04	0.04	0.04	0.04
3 versus 1	0.13	0.14	0.14	0.13	0.14	0.13
2 versus 1	0.12	0.12	0.12	0.11	0.12	0.11

Table 6 – Progression classification in trials with a low response rate: proportion of patients classified discordantly into progressors and non-progressors.

Number of lesions being compared	N = 25		N = 50		N = 100	
	Radiologist 1	Radiologist 2	Radiologist 1	Radiologist 2	Radiologist 1	Radiologist 2
10 versus 5	0.02	0.02	0.02	0.02	0.02	0.02
10 versus 3	0.03	0.04	0.04	0.03	0.04	0.04
10 versus 2	0.05	0.06	0.06	0.05	0.05	0.05
10 versus 1	0.10	0.10	0.10	0.10	0.10	0.09
5 versus 3	0.03	0.03	0.03	0.03	0.03	0.03
5 versus 2	0.05	0.05	0.05	0.05	0.05	0.05
5 versus 1	0.09	0.09	0.09	0.09	0.09	0.09
3 versus 2	0.04	0.04	0.04	0.04	0.04	0.04
3 versus 1	0.09	0.09	0.08	0.08	0.08	0.08
2 versus 1	0.08	0.08	0.07	0.07	0.07	0.07

Table 7 – Response classification in trials with a high response rate: proportion of patients classified discordantly into responders and non-responders.

Number of lesions being compared	N = 25		N = 50		N = 100	
	Radiologist 1	Radiologist 2	Radiologist 1	Radiologist 2	Radiologist 1	Radiologist 2
10 versus 5	0.01	0.01	0.01	0.01	0.01	0.01
10 versus 3	0.03	0.03	0.03	0.03	0.03	0.03
10 versus 2	0.06	0.05	0.05	0.05	0.05	0.05
10 versus 1	0.12	0.11	0.12	0.12	0.12	0.12
5 versus 3	0.02	0.02	0.02	0.02	0.02	0.02
5 versus 2	0.05	0.05	0.05	0.05	0.05	0.05
5 versus 1	0.11	0.11	0.11	0.12	0.11	0.11
3 versus 2	0.04	0.03	0.04	0.04	0.04	0.04
3 versus 1	0.10	0.10	0.11	0.11	0.11	0.11
2 versus 1	0.09	0.09	0.09	0.09	0.09	0.09

Table 8 – Progression classification at a single time point in trials with a high response rate: proportion of patients classified discordantly into progressors and non-progressors.

Number of lesions being compared	N = 25		N = 50		N = 100	
	Radiologist 1	Radiologist 2	Radiologist 1	Radiologist 2	Radiologist 1	Radiologist 2
10 versus 5	0.02	0.02	0.01	0.01	0.01	0.01
10 versus 3	0.03	0.03	0.03	0.03	0.03	0.03
10 versus 2	0.04	0.04	0.04	0.04	0.04	0.04
10 versus 1	0.07	0.07	0.07	0.07	0.07	0.07
5 versus 3	0.02	0.02	0.02	0.02	0.02	0.02
5 versus 2	0.03	0.03	0.03	0.03	0.03	0.03
5 versus 1	0.06	0.06	0.06	0.06	0.06	0.06
3 versus 2	0.02	0.02	0.02	0.02	0.02	0.02
3 versus 1	0.06	0.06	0.06	0.06	0.06	0.06
2 versus 1	0.05	0.05	0.05	0.05	0.05	0.05

across trials with low and high response rates as well as patients with low and high response probabilities. Measuring five lesions results in a very small loss of information, whereas measuring fewer lesions may not sufficiently capture patient response.

In all our analyses, we used the largest lesions based on our actual size, effectively assuming that the radiologist always chooses the ‘correct’ lesions based on a size criterion. In practice, this theoretically would require measuring all

the lesions first, which defies the purpose of lesion selection. Therefore, our results are optimistic estimates of error introduced by measuring a smaller number of lesions. In practice, we can see even higher biases in estimating the response rate and higher rates of misclassified patients as radiologists occasionally fail to include the largest lesions according to their visual inspection, or purposely may not include the largest lesions because they feel that a particular lesion may not be reproducibly measurable.

There are some limitations of this simulation study. The results depend on a model which required several assumptions. The assumptions we made (such as the normality of the tumour measurements on the natural logarithm scale and the correlation structure) may deviate from the truth. Thus, the simulated lesion measurements may not precisely represent true lesion measurements in clinical trials. However, it is important to keep in mind that our goal was not to perfectly model how tumours change over time, but rather to have a sensible approximation that would allow us to assess the affect of the number of lesions on trial-level summary statistics such as the response rate. It is often said that all models are wrong but some are useful.¹⁰ Based on our analysis of actual lesion measurements, we believe that the model used in this simulation study is reasonable and useful for the stated purposes of the study.

Our model simulates lesion measurements at only two time points. This approach allows us to assess how the number of lesions affects the estimates of the proportion of patients responding to a treatment and the proportion of patients having progressive disease. This approach, however, does not allow us to look or conclude about optimising the number of lesions for time-to-event outcomes such as time to progression or progression-free survival. Generating data at more than two time points is extremely complex due to the multiple possible variants in lesion growth curves in the presence of a treatment. For instance, lesions may respond to treatment and continually shrink, or they may initially respond but then begin to grow again. Alternatively, lesions may not respond to treatment and continue to grow over time. These scenarios are just several possibilities. Attempting to model this process (and in addition determining the proportion of lesions that behave in a particular fashion) is beyond the scope of this paper. It remains an important question; however, as more and more trials use progression-free survival as their primary end-point.

The third issue to be considered is that our definition of progressive disease is limited by the fact that we only considered the effect of lesions that were present at a baseline measurement. In clinical practice and in clinical trials, patients are assessed not only based upon the target lesions, but also upon the non-target disease and the development of new lesions. The impact that non-target assessment, which is generally very qualitative, and new lesions, which may or may not be recognised as new metastatic disease, will have on the concordance of disease progression is uncertain.

Finally, we did not consider a model in which patient response is a predictor of overall survival. If, as we argued above, generating longitudinal measurements is much more complex than a snapshot in time, capturing what happens beyond progression in a simulation study is even more complicated by factors such as salvage therapy, age and co-morbid conditions and toxicities resulting from the initial treatment. Nevertheless, this is also an interesting question that could be considered in the future, preferably starting with the analysis of large randomised trials.

The use of tumour measurements extends beyond RECIST.¹¹ Increasingly, investigators use measurements in waterfall analyses and evaluate responses, progressions and simply change in tumour size as a continuous variable.¹²

The use of tumour measurements in this regard may dictate even stricter requirements for concordance and therefore the need to measure more lesions or measure lesions more accurately. Based upon the existing data and current contemporary use of tumour measurements in RECIST, it appears that decreasing the number of lesions measured to five is a satisfactory compromise between capturing 'total' tumour burden and the resource commitment needed to accomplish this goal both for a single patient and for a clinical trial. This variable, however, will need to be continually re-evaluated with changes in therapies, in modalities used to assess these therapies and in metrics or response criteria used to categorise the benefit of the therapy.

Conflict of interest statement

None declared.

Acknowledgements

The authors would like to thank the members of the RECIST International Working Group for their comments during the development of the model. In particular, we are grateful to Dr. Lori Dodd for her helpful suggestions. We are also thankful to Ms. Joanne Chou for preparing the data warehouse used to obtain input values to the simulation model. This work was supported in part by Grant NIH R01 CA125143 and by funding from the Experimental Therapeutics Center of Memorial Sloan-Kettering Cancer Center.

Appendix A

Model

In each simulation set, we simulated data for 1000 hypothetical Phase II studies. For each Phase II study in the same simulation set, we generated data on N patients with 10 lesions. We specified that based on the measurements from 10 lesions a proportion of the patients were responders, denoted by $Z = 2$; a proportion were progressors, denoted by $Z = 1$ and a proportion had stable disease, denoted by $Z = 0$. To generate lesion measurements, we used a mixture of three mixed-effects models that allowed parameter values to differ between responders, progressors and patients who were neither responding nor progressing:

$$\begin{aligned} \ln(y_{ijkt}) = & I(Z_i = 0) \times \left(\delta_t^{(Z=0)} + \lambda_i^{(Z=0)} + \alpha_{j(i)}^{(Z=0)} + \epsilon_{ijkt}^{(Z=0)} \right) \\ & + I(Z_i = 1) \times \left(\delta_t^{(Z=1)} + \lambda_i^{(Z=1)} + \alpha_{j(i)}^{(Z=1)} + \epsilon_{ijkt}^{(Z=1)} \right) \\ & + I(Z_i = 2) \times \left(\delta_t^{(Z=2)} + \lambda_i^{(Z=2)} + \alpha_{j(i)}^{(Z=2)} + \epsilon_{ijkt}^{(Z=2)} \right) + \beta_k \end{aligned}$$

where $i = 1, \dots, N$; $j = 1, \dots, 10$; $k = 1, 2$; $t = 0, 1$. In this model, y_{ijkt} is the lesion measurement for the i th patient, j th lesion, at time t , as measured by the k th radiologist. Time $t = 0$ represents a baseline measurement, whilst time $t = 1$ represents a follow-up measurement. The model specifies that y_{ijkt} is a function of five components where the values of all the components except for one, β_k , depend on the value of Z :

- (1) $\delta_i^{(Z=0)}$ is a fixed effect that represents the overall mean lesion measurement amongst responders at time t . Similarly, $\delta_i^{(Z=1)}$ and $\delta_i^{(Z=2)}$ represent the overall mean lesion measurement at time t amongst patients with progression and stable disease, respectively.
- (2) $\lambda_i^{(Z=0)}$, $\lambda_i^{(Z=1)}$ and $\lambda_i^{(Z=2)}$ are the subject random effects for responders, progressors, and patients with stable disease, respectively. We assume $\lambda_i^{(Z=0)} \sim \text{Normal}(0, \sigma_{\lambda(Z=0)}^2)$, $\lambda_i^{(Z=1)} \sim \text{Normal}(0, \sigma_{\lambda(Z=1)}^2)$ and $\lambda_i^{(Z=2)} \sim \text{Normal}(0, \sigma_{\lambda(Z=2)}^2)$.
- (3) $\alpha_{j(i)}^{Z=0}$, $\alpha_{j(i)}^{Z=1}$ and $\alpha_{j(i)}^{Z=2}$ are the lesion random effects, which are nested within subject. We assume $\alpha_{j(i)}^{Z=0} \sim \text{Normal}(0, \sigma_{\alpha(Z=0)}^2)$, $\alpha_{j(i)}^{Z=1} \sim \text{Normal}(0, \sigma_{\alpha(Z=1)}^2)$ and $\alpha_{j(i)}^{Z=2} \sim \text{Normal}(0, \sigma_{\alpha(Z=2)}^2)$.
- (4) $\varepsilon_{ijkt}^{(Z=0)}$, $\varepsilon_{ijkt}^{(Z=1)}$ and $\varepsilon_{ijkt}^{(Z=2)}$ are the random error terms with $\varepsilon_{ijkt}^{(Z=0)} \sim \text{Normal}(0, \sigma_{\varepsilon(Z=0)}^2)$, $\varepsilon_{ijkt}^{(Z=1)} \sim \text{Normal}(0, \sigma_{\varepsilon(Z=1)}^2)$ and $\varepsilon_{ijkt}^{(Z=2)} \sim \text{Normal}(0, \sigma_{\varepsilon(Z=2)}^2)$.
- (5) β_k is the radiologist random effect. We assume that this random effect is distributed similarly amongst all simulated patients and that $(\beta_1, \beta_2)^T \sim \text{Multivariate Normal}(0, \Sigma_\beta)$ where the components of Σ_β are σ_β^2 on the diagonal and $\sigma_{\beta 12}$ on the off-diagonal.

The natural logarithm of each lesion measurement is then determined by summing across each of these component pieces. We use the natural logarithm of the lesion measurements because in our experience with analysis of real data sets, we have found that the logarithm of the measurement is more reasonably approximated by a normal distribution than are the raw, untransformed measurements.

After the lesion measurements have been generated according to this model, measurements were summed across lesions within patient for each time point and radiologist. The relative percent change from baseline to follow-up was calculated for the two radiologists. That is,

$$R_{ik} = 100 \times \frac{\sum_{j=1}^J y_{ijk1} - \sum_{j=1}^J y_{ijk0}}{\sum_{j=1}^J y_{ijk0}}$$

is the relative percent change in tumour burden for the i th patient, k th reading. This yielded N pairs, (R_{11}, R_{12}) , (R_{21}, R_{22}) , ..., (R_{N1}, R_{N2}) , of measured changes in tumour sizes. For each patient, there are two response assessments arising from the two radiologists. We were primarily interested in calculating the change within radiologist. In other words, our primary focus was on the relative change from baseline to follow-up for the first radiologist and then separately for the second radiologist, rather than studying the relative change from baseline, radiologist 1 to follow-up radiologist

2, for instance. The R_{ik} were then divided into response categories using the definitions from RECIST. A complete response (CR) was defined by $R_{ik} = -100$, whilst a partial response was defined as $-100 < R_{ik} \leq -30$. $R_{ik} \geq 20$ denoted progressive disease (PD) and $-30 \leq R_{ik} \leq 20$ denoted stable disease (SD).

After response has been assessed using the measurements from 10 lesions, subsets of the 10 lesions were selected and analysed for each patient. For each patient, the S largest lesions as measured by the k th radiologist at the baseline measurement were selected. That is, the lesions that are selected to be included in the subsets may differ between the two radiologists. Response assessment was calculated as above based only on the S lesions whilst ignoring the remaining lesions.

Simulations were performed in the statistical software package R (copyright: The R Foundation for Statistical Computing).

Parameter values

We aimed to simulate data that would show the affect of decreasing the number of lesions measured first in Phase II studies with a substantial treatment effect and then in Phase II studies with a smaller treatment effect. In order to obtain parameter values to be used in the simulation model, we analysed existing data from actual studies on real patients.

Values for $\delta_i^{(Z=0)}$, $\delta_i^{(Z=1)}$, $\delta_i^{(Z=2)}$, $\sigma_{\lambda(Z=0)}^2$, $\sigma_{\lambda(Z=1)}^2$, $\sigma_{\lambda(Z=2)}^2$, $\sigma_{\alpha(Z=1)}^2$, $\sigma_{\alpha(Z=2)}^2$, $\sigma_{\varepsilon(Z=0)}^2$, $\sigma_{\varepsilon(Z=1)}^2$ and $\sigma_{\varepsilon(Z=2)}^2$ were obtained from several of the trials from the data warehouse that were independently reviewed ('New response evaluation criteria in solid tumors: revised RECIST guideline (version 1.1)'). We fit mixed-effects models using the method of restricted maximum likelihood¹³ separately to responders, progressors and patients with stable disease for each of the eight protocols included in the data set and obtained eight sets of estimates for each of the above parameters. The PROC MIXED procedure in SAS (version 9.1 for Windows, The SAS Institute Inc.) is used for this purpose.

We combined estimates using weighted averages of the protocol-specific estimates, first averaging over protocols with a more substantial treatment effect and then separately averaging over protocols with a smaller treatment effect. We focused on using the same progression rate in both instances, and again obtained parameter estimates by taking weighted averages over protocols with similar progression rates. Based on this analysis, we simulated data with a low progression rate and a response rate that was either moderately low or relatively high. Additional results of this analysis detailing the parameter values that we used to simulate data are contained in Table 9.

Table 9 – Parameter values used in simulation model.

	δ_0	δ_1	σ_{λ}^2	σ_{α}^2	σ_{ε}^2	σ_{β}^2	$\sigma_{\beta 12}$
Responders ($Z = 0$, low response)	3.10	2.43	0.06	0.11	0.03	0.003	0.001
Responders ($Z = 0$, high response)	3.10	2.34	0.16	0.19	0.18	0.003	0.001
Progressors ($Z = 1$)	3.10	3.36	0.13	0.21	0.06	0.003	0.001
Patients with stable disease ($Z = 2$)	3.10	3.08	0.12	0.15	0.03	0.003	0.001

Values for σ_β^2 and $\sigma_{\beta12}$ were obtained by fitting a random effects model to data collected for a separate study looking at the reproducibility of CT measurements. These data are described in detail elsewhere.¹⁴ The parameter estimates that resulted from this analysis and were used to generate data for our simulation study are also contained in Table 9.

Within each set of simulations, we generated data for a fixed number of patients, N , for each hypothetical Phase II study. We used the values of 25, 50 and 100 for N across different sets of simulations. We studied the affect on the estimates of response and progression when $S = 5, 3, 2$ and 1 target lesions were measured in comparison to when 10 target lesions were measured.

REFERENCES

1. Therasse P, Arbuck SG, Eisenhauer EA, Wanders J, Kaplan RS, Rubinstein L, et al. New guidelines to evaluate the response to treatment in solid tumors. European Organization for Research and Treatment of Cancer, National Cancer Institute of the United States, National Cancer Institute of Canada. *J Natl Cancer Inst* 2000;**92**(3):205–16.
2. Schwartz LH, Mazumdar M, Brown W, Smith A, Panicek DM. Variability in response assessment in solid tumors: effect of number of lesions chosen for measurement. *Clin Cancer Res* 2003;**9**(12):4318–23.
3. Miller AB, Hoogstraten B, Staquet M, Winkler A. Reporting results of cancer treatment. *Cancer* 1981;**47**(1):207–14.
4. WHO handbook for reporting results of cancer treatment. Geneva (Switzerland): World Health Organization Offset Publication No. 48; 1979.
5. Hopper KD, Kasales CJ, Van Slyke MA, Schwartz TA, TenHave TR, Jozefiak JA. Analysis of interobserver and intraobserver variability in CT tumor measurements. *AJR Am J Roentgenol* 1996;**167**(4):851–4.
6. Schwartz LH, Ginsberg MS, DeCorato D, et al. Evaluation of tumor measurements in oncology: use of film-based and electronic techniques. *J Clin Oncol* 2000;**18**(10):2179–84.
7. Bogaerts J, Ford R, Sargent D, et al. Individual patient data analysis to assess modifications to the RECIST criteria. *Eur J Cancer* 2009;**45**:248–60.
8. Fleiss JL, Levin B, Paik MC. *Statistical methods for rates and proportions*. New York: John Wiley and Sons Inc.; 2003.
9. Simon R. Optimal two-stage designs for phase II clinical trials. *Control Clin Trials* 1989;**10**(1):1–10.
10. Box GEP, Draper NR. *Empirical model-building and response surfaces*. New York: John Wiley and Sons Inc.; 1987.
11. Eisenhauer EA, Therasse P, Bogaerts J, et al. New response evaluation criteria in solid tumors: Revised RECIST guideline (version 1.1). *Eur J Cancer* 2009;**45**:228–47.
12. Karrison TG, Maitland ML, Stadler WM, Ratain MJ. Design of phase II cancer trials using a continuous endpoint of change in tumor size: application to a study of sorafenib and erlotinib in non small-cell lung cancer. *J Natl Cancer Inst* 2007;**99**(19):1455–61.
13. Harville DA. Maximum likelihood approaches to variance component estimation and to related problems. *J Am Stat Assoc* 1977;**72**(358):320–38.
14. James LP, Zhao B, Moskowitz CS, et al. Reproducibility of computed tomography (CT) measurements of lung cancer. *J Clin Oncol* 2008;**26**(Suppl.) [Abstract 8002].